

The use of oscillatory signals in the study of genetic networks

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Edited by Charles S. Peskin, New York University, New York, NY, and approved March 18, 2005 (received for review May 27, 2004)

The structure of a genetic network is uncovered by studying its response to external stimuli (input signals). We present a theory of propagation of an input signal through a linear stochastic genetic network. We found that there are important advantages in using oscillatory signals over step or impulse signals and that the system may enter into a pure fluctuation resonance for a specific input frequency.

systems biology | synthetic biology | stochastic processes

The nature of a physical system is revealed through its response to external stimulation. The stimulus is imposed on the system, and its effects are then measured (Fig. 1*a*). This approach is widely used in biology: a cell culture is perturbed with a growth factor, a heat shock, etc. The data measured contain the initial information encoded into the stimulus and the information about the intrinsic characteristics of the system. The more parameters the experimentalist can adjust to craft the perturbation stimulus, the more information about the system can be revealed. In recent years we have witnessed a tremendous increase in measurement capabilities (e.g., microarray and proteomic technologies, better reporter genes). However, the success of the systems approach to molecular biology depends not only on the measurement instruments, but also on an effective design and implementation of the input stimulus, which has not been thoroughly explored. Traditionally, two types of time-dependent stimuli are at work in molecular biological experiments (1, 2). For example, a step stimulus is obtained when at one instant of time a growth factor is added to the medium (Fig. 1*a*, graph *a*). The stimulus from graph *b* in Fig. 1*a* is a superposition of two step stimuli. The investigator can control the height of the step stimulus (the concentration of the growth factor) or the time extension of the heat shock. The cells respond to these stimuli only transiently. The response is dampened after some time and becomes harder to detect because of noise. To overcome the noise, the concentration of the stimulus is typically increased to the point where the strength of the stimulus raises far above its physiological range.

We propose to implement a molecular switch at the level of gene promoter and use it to impose an oscillatory stimulus. In the absence of experimental noise, any stimulus can be used to determine the input-output properties of a genetic network. However, in the presence of experimental noise, oscillatory input has many advantages: (i) the measurements can be extended to encompass many periods so the signal-to-noise ratio can be dramatically improved; (ii) the measurement can start after transient effects subside, so that the data become easier to incorporate into a coherent physical model; and (iii) an oscillatory stimulus has more parameters (period, intensity, slopes of the increasing and decreasing regimes of the stimulus) than a step stimulus. As a consequence, the measured response will contain much more quantitative information. Experimental results from neuroscience prove that oscillatory stimulus can modulate the mRNA expression level of genes. For example, the *c-fos* transcription level in cultured neurons is enhanced 400% by an electrical stimulus at 2.5 Hz and reduced by 50% at 0.01 Hz

(3). Also, the mRNA levels of cell recognition molecule L1 in cultured mouse dorsal root ganglion neurons change if the frequency of the electric pulses is varied. The expression level of L1 decreases significantly after 5 days of 0.1-Hz stimulation but not after 5 days of 1-Hz stimulation (4). To extend the oscillatory approach to other types of cells, a two-hybrid assay (5) can be used to implement a molecular periodic signal generator (Fig. 1*c*). The light switch is based on a molecule (phytochrome in ref. 5) that is synthesized in darkness in the Q1 form. When the Q1 form absorbs a red light photon (wavelength 664 nm) it is transformed into the form Q2. When Q2 absorbs a far red light (wavelength 748 nm) the molecule Q goes back to its original form, Q1. The transitions take milliseconds. The protein P interacts only with the Q2 form, thus recruiting the activation domain to the target promoter. In this position, the promoter is open and the gene is transcribed. After the desired time has elapsed, the gene can be turned off by a photon from a far red light source. Using a sequence of red and far red light pulses the molecular switch can be periodically opened and closed.

There are four input parameters that can be varied: the period (*T*), the time separation between the pulses (*s*), and the amplitude (*A*) of the red and the far red pulses. The mRNA concentration profile will depend on these parameters and can be measured with high-throughput technology (6). Protein levels also will depend on the input signal. The proteins can be recorded with 2D PAGE analysis or MS. If one single gene product is targeted, then a real-time luminescence recording can be used (7). A periodic generator can be used to investigate biological systems for which the mRNA and protein concentrations naturally oscillate in time. An example of such a system is the circadian clock that drives a 24-h rhythm in living organisms from human to cyanobacteria. The core oscillator is a molecular machinery based on an autoregulatory feedback loop involving a set of key genes (*Bmal*, *Per1*, *Per2*, *Per3*, *Cry1*, *Cry2*, etc.) (8). Experimental procedures used to elucidate the clock mechanism are based on measuring the circadian wheel-running behavior of mice under normal light/dark cycles or in constant darkness (dark/dark) conditions. Experimental evidence demonstrates that laws of quantitative nature govern the molecular clock. For example (9), the internal clock of *Cry1* mutants have a free-running (i.e., dark/dark conditions) period of 22.51 ± 0.06 h, which is significantly lower than the period of 23.77 ± 0.07 h for WT mice. In contrast, a *Cry2* mutant has a significantly higher period of 24.63 ± 0.06 h. In light/dark conditions, both mutants follow the 24-h period of the entrained light cycles. A double *Cry1,2* mutant is arrhythmic in dark/dark conditions and follows a 24-h rhythm in light/dark conditions. To explain these experimental values we suggest using a light-switchable generator to drive the expression level of *Cry1* and *Cry2* and measure the dynamics of transcription and the translation for the rest of the key clock genes. Another application of the periodic generator is to modulate a constitutively expressed gene by superimposing an oscillatory profile on top of its

This paper was submitted directly (Track II) to the PNAS office.

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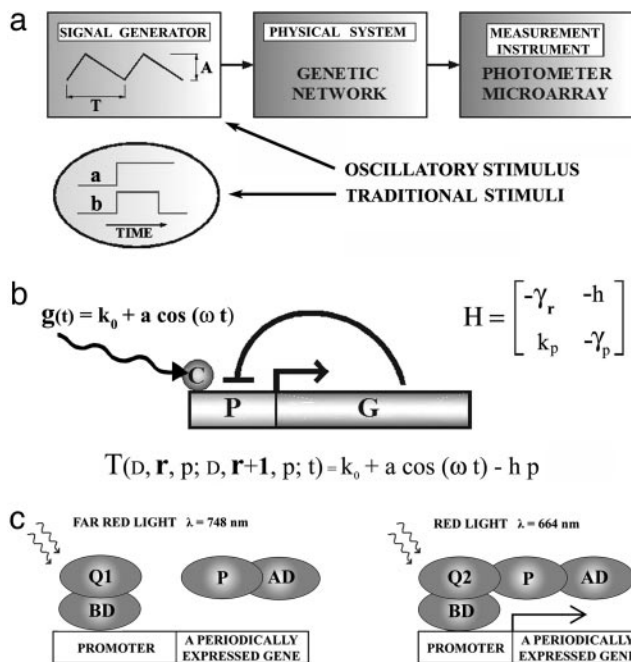


Fig. 1. Genetic networks stimulated by signal generators. (a) Genetic network response depends on the type of the applied stimulus. (b) An autoregulatory network. The gene G is under the influence of a cofactor C that rhythmically modulates the activity of the promoter P . The matrix H contains the parameters that dictate the transition probabilities of the stochastic model. The transition probability per unit time from r to $r + 1$ mRNA molecules, $T(D, r, p; D, r + 1, p; t)$, is modulated by the oscillatory signal generator. The DNA, D , and the protein, p , do not change in this transition. (c) The gene is turned on with a red light pulse of wavelength $\lambda = 664$ nm. With a far red light of wavelength $\lambda = 748$ nm the gene is turned off. Adapted from ref. 5. AD, activation domain; BD, binding domain; Q, a protein that changes its form upon light exposure, from Q1 to Q2 and back; P, a protein that interacts only with form 2 of protein Q (Q2).

flat level. Then, the genes that show a modulation with a frequency equal to the generator's frequency will be detected by a microarray experiment. Why is this approach different from the one where a step stimulus is used? Because the frequency of the generator is not an internal parameter of the biological system. The genes that interact with the driven gene will be modulated by the input frequency. The rest of the genes will have different expression profiles dictated by the internal parameters of the biological system. This point of view is supported by our findings (6) that the circadian clock (which is an endogenous periodic signal generator) propagates its output to only 8–10% of the transcriptome in mice peripheral tissues (liver or heart). In contrast to the oscillatory input, when a step stimulus is applied, all of the expression profiles are dictated by the internal parameters of the biological system. Except for the height of the step stimulus (the dose of the factor applied) there is no external parameter implemented into the input signal. As such, it is difficult to separate those genes that directly respond to the input signal and consequently avoid artifacts. With the applications described in mind, we study the propagation of an input signal through a stochastic genetic network.

The Response of a Stochastic Genetic Network to an Input Stimulus

The effects of an oscillatory input have been studied on specific biological systems by using models based on differential equations (10–12). The stochastic character is embedded into these equations as an exterior additive term. In contrast, we compute the generator's effects on the mean and fluctuation of the gene products with

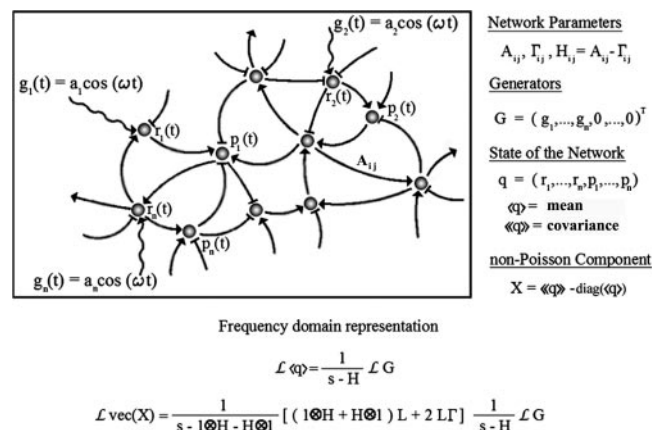


Fig. 2. Response of a stochastic genetic network to an oscillatory input. The Laplace transform \mathcal{L} changes the dynamic variable from time to frequency. In the $\text{vec}(X)$ all of the elements of matrix X are arranged in a column vector.

a stochastic model (13–15). In this way, the generated stimulus and the noisy nature of the cell are entangled in the stochastic genetic model. For a network of n genes (Fig. 2) the state of a cell is described by the mRNA and protein molecule numbers: $q = (r_1, \dots, r_n, p_1, \dots, p_n)$. We assume that, during any small time interval Δt , the probability for the production of a molecule of the i th type is $(\sum_{j=1}^n A_{ij} q_j + G_i(t)) \Delta t$, i.e., q_i is increased by 1 with the above probability. The function $G_i(t)$ represents the time-varying input signal and modulates the mRNA production only: $G = (g_1(t), \dots, g_n(t), 0, \dots, 0)^T$ (the superscript T is the transposition operation that transforms G into a column vector for notational convenience in what follows). The parameter A_{ij} represents the influence of the j th type of molecule on the production rate of a molecule of the i th type. Similarly, there is a matrix of parameters Γ_{ij} governing the degradation rates of the molecules. For simplicity, we assume that the input stimulus directly affects only the production rates. The mean $\mu = \langle q \rangle$ and the covariance matrix $\nu = \langle\langle q \rangle\rangle = \langle\langle (q - \langle q \rangle)(q - \langle q \rangle)^T \rangle\rangle$ of the state q are driven by the generator G .

The transfer of the signal from the generator through the genetic network to the output measured data is encapsulated in a set of transfer matrices. Specifically, let $H = A - \Gamma$ and denote the Laplace transforms of μ and G by $L\mu$ and LG . Here and in what follows, μ and G are represented as column vectors. The connection between the mean and the generators is given by formula 1, which is typical for a deterministic linear system. However, the genetic system is stochastic and the measure of the intrinsic noise is quantified by the covariance matrix ν . The effect of the stimulus generators is most transparent if we split ν in a Poisson and a non-Poisson component: $\nu = \text{diag}(\mu) + X$. Here $\text{diag}(\mu)$ represents a matrix with the components of the vector μ on its diagonal, with all of the other terms being zero. For a Poisson process, $X = 0$ and thus the term $\text{diag}(\mu)$ is called the Poisson component of ν . The non-Poisson component $X = \nu - \text{diag}(\mu)$ can be expressed in terms of the generators (Appendix and Supporting Text, which is published as supporting information on the PNAS web site):

$$L\mu = \frac{1}{(s - H)} LG, \quad [1]$$

$$L\text{vec}(X) = \frac{1}{s - 1 \otimes H - H \otimes 1} [-(1 \otimes H + H \otimes 1)L + 2LG] \frac{1}{s - H} LG. \quad [2]$$

The $\text{vec}(X)$ is a vector constructed from the matrix X by stripping the columns of X one by one and stacking them one on top of each other in $\text{vec}(X)$. We emphasize here that the time variation of the generators G in **2** can take any form and is not bounded to be periodic or a step stimulus.

There are three matrices that transfer the information from the generators to the non-Poisson component, $L\text{vec}(X) = M_3 M_2 M_1 L G$. The first, $M_1 = (s - H)^{-1}$, is the same as the transfer matrix for the mean. The second, $M_2 = (1 \otimes H + H \otimes 1)L + 2L\Gamma$, breaks the symmetry between the degradation and production parameters that are otherwise hidden in the matrix $H = A - \Gamma$. The \otimes is the Kronecker product of two matrices. The matrix L (with elements 0 and 1) is the lifting matrix from dimension of the mean ($2n$ values) to the dimension of $\text{vec}(X)$ ($4n^2$ values). The third matrix is $M_3 = (s - 1 \otimes H - H \otimes 1)^{-1}$. If λ_i is the eigenvalue of H then all combinations $\lambda_i + \lambda_j$ are the eigenvalues of $1 \otimes H + H \otimes 1$. Thus M_3 represents the analog of M_1 in the space of covariance variables.

For a step stimulus, these eigenvalues are of primal importance: the measured signal is a superposition of components with different eigenvalues and has a complicated mathematical expression. However, for a periodic stimulus, the frequency of the external generator is the important parameter. This frequency is fixed by the experimentalist not by the biological system. Only the phase and the amplitude of the output signal depends on the system's eigenvalues and the mathematical form is less cumbersome than for the step stimulus. The input-output relations, **1** and **2**, were derived from the master equation written for the probability of the states of the genetic network. Thus, we must specify the initial conditions for the probability of the states. These conditions refer here to states for which one molecular component vanishes ($q_i = 0$, for one i). The input-output relations, **1** and **2**, are independent of these boundary states if the Γ matrix is diagonal. A diagonal Γ matrix was used in ref. 13, and we will use it also in the example that follows. Tools developed in the field of system identification can be used to create models for the networks under study (16). The difference between the system identification classical models and a genetic network is that the latter is a stochastic process by nature, whereas the former are deterministic models with a superimposed noise from external sources. However, the formulas that describe the relations between the mean and covariance of the stochastic process and the input signals, **1** and **2**, are of the same general nature as those used in system identification theory (16). In the next section we will use **1** and **2** to analyze one of the most fundamental regulatory motifs in a genetic network: an autoregulatory gene that acts upon itself through a negative feedback (17–19). The fluctuation can drive this biological system out of its equilibrium state (20).

Fluctuation Resonance

Four parameters characterize the system: the feedback strength $A_{12} = -h$, the translation rate $A_{21} = k_p$, and two degradation rates, $\Gamma_{11} = \gamma_r$, $\Gamma_{22} = \gamma_p$. The gene regulation is under the control of its own protein product and the protein activity is modulated by a cofactor. The cofactor is driven by a periodic light-switchable generator $g(t) = k_0 + a \cos(\omega t)$ (Fig. 1a). Before the generator is applied, the transcription rate is equal with k_0 and the system is in a steady state. Through the transfer matrices, **1** and **2**, the light generator will impose a periodic evolution of the mean and covariance matrix for mRNA and protein product. We denote the mean mRNA by $\langle r(t) \rangle$ and the mean number of protein by $\langle p(t) \rangle$. We will concentrate on the protein number in what follows. After the transients are gone, $\langle p(t) \rangle = P_0 + P_1 e^{i\omega t} + P_1^* e^{-i\omega t}$, that is the protein number will oscillate with an amplitude P_1 on top of a baseline P_0 ; here $*$ represents complex conjugation. The fluctuation of the protein number, $\langle\langle p(t) \rangle\rangle$, differs from the mean number by a quantity that we denoted by

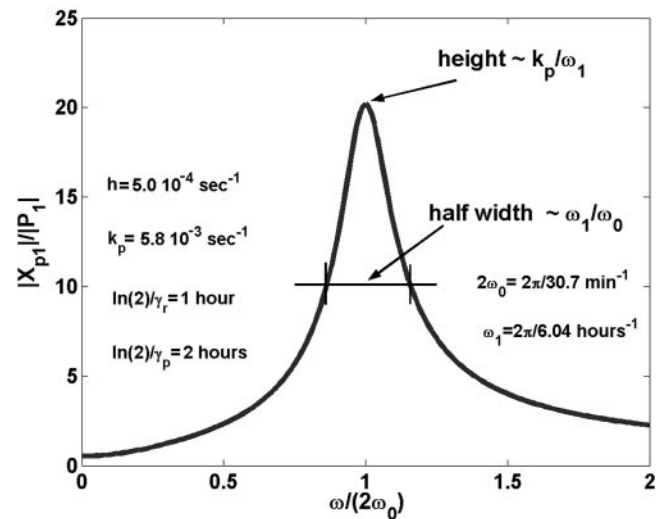


Fig. 3. Fluctuation resonance. The amplitude $X_{p,1}$ of the non-Poisson component is much higher than the amplitude of the mean protein number, P_1 , at $\omega = 2\omega_0$.

$X_{pp}(t)$: $\langle\langle p(t) \rangle\rangle = \langle p(t) \rangle + X_{pp}(t)$. For a pure Poisson process, $\langle\langle p(t) \rangle\rangle = \langle p(t) \rangle$. Thus the term $X_{pp}(t)$ represents the deviation from a Poisson process. If there is some information about the genetic system that can be uncovered by measuring not only the mean but also the covariance matrix, then this information is hidden only in the non-Poisson component $X_{pp}(t)$. The quantity $X_{pp}(t)$ is not interesting only from a statistical point of view but also from a dynamical one. The equation for the time evolution of $\langle\langle p(t) \rangle\rangle$ takes its most simple form if it is written for $X_{pp}(t)$. That is, the time dependence of the mean value must be subtracted from the time evolution of $\langle\langle p(t) \rangle\rangle$. Similar to the mean value, the non-Poisson component of the fluctuation will oscillate in time, $X_{pp}(t) = X_{p,0} + X_{p,1} e^{i\omega t} + X_{p,1}^* e^{-i\omega t}$ with complex amplitude $X_{p,1}$. The relative strength of the fluctuation versus the mean value can be described by using the Fano factor (13): $\langle\langle p(t) \rangle\rangle / \langle p(t) \rangle = 1 + X_{pp}(t) / \langle p(t) \rangle$. For oscillatory inputs, the response of the network is best described in frequency domain rather than in time. In frequency domain, as an analog of the Fano factor we consider the ratio of the amplitude of $X_{pp}(t)$ versus the amplitude of $\langle p(t) \rangle$.

$$\frac{|X_{p,1}|}{|P_1|} = \left(4k_p^2 \frac{(\omega^2 + (h - \gamma_p)^2)(\omega^2 + 4\gamma_r^2)}{((\omega^2 - 4\omega_0^2)^2 + 4\omega^2\omega_1^2)(\omega^2 + \omega_1^2)} \right)^{1/2} \quad [3]$$

Here $\omega_1 = \gamma_r + \gamma_p$. The complex amplitudes $X_{p,1}$ and P_1 depend on the input frequency, and therefore resonance phenomena can be detected in the system. If the light-switchable generator oscillates with double the natural frequency $\omega_0^2 = hk_p + \gamma_r\gamma_p$, that is, $\omega = 2\omega_0$ we find a state of resonance for fluctuation and not for the mean (Fig. 3).

For $\omega = 2\omega_0$ the system will be in a pure fluctuation resonance. In such a situation the molecular noise can drive the cell out of its equilibrium state, which can have dramatic consequence on the cell fate. Our model being linear cannot cover the entire phenomena that accompanies a system whose state is close to resonance. However, a linear model suggests the existence of pure fluctuation resonance. At fluctuation resonance, the deviation from a Poissonian process is high. The oscillation amplitude for protein fluctuation is much greater than the amplitude of the mean. Experimental results (21) show that typical values for the ratio k_p/γ_r are 40 for *lacZ* and 5 for *lacA*. These values

suggest that there are natural conditions for a strong height fluctuation resonance (Fig. 3). However, for a sharp fluctuation resonance (small half width), we need $h > \gamma_r$ or γ_p , a condition that does not appear in all genetic networks. It is through the experimental study that we will clarify how some biological systems can sustain fluctuation resonance and others can not. Besides resonance, the frequency response provides other insights into the structure of the autoregulatory system. The parameters of the system can be read from the measured data. The frequency response of the mean values behave like the response of a classical linear system to input signals. The new aspects are those related to fluctuations. Like $X_{pp}(t)$ and $X_{rr}(t)$, the correlation coefficient between the mRNA and protein number will oscillate in time: $X_{rp}(t) = X_{rp,0} + X_{rp,1}e^{i\omega t} + X_{rp,1}^*e^{-i\omega t}$ with amplitude $X_{rp,1}$. Taking the ratios of the amplitudes $|X_{rp,1}|^2/|X_{r,1}|^2 = (1/4h^2)\omega^2 + \gamma_r^2/h^2$, $|X_{rp,1}|^2/|X_{p,1}|^2 = (1/4k_p^2)\omega^2 + \gamma_p^2/k_p^2$, we observe that all four parameters of the system can be estimated from the slopes and the intercepts of the above ratios as a function of ω^2 . Detail formulas for each amplitude are given in *Supporting Text*.

The Spectrum, the Experimental Noise, and the Importance of the Input Stimulus

We described the use of a periodic signal to decipher a genetic network. Traditionally, a step stimulus is used in biology for pathway detection (i.e., adding a growth factor to the culture). From the response to a step stimulus we can extract, in principle, the parameters of the system. The natural question is then: why should we generate a periodic stimulus when there is already a step stimulus in use? Seeking an answer, we notice that the measured data in our studied example can be expressed as a sum of exponentially decaying functions, $e^{-\lambda t}$, if a step stimulus was used (*Supporting Text*). For a periodic input, the response contains only exponentials with imaginary argument, $e^{i\omega t}$. Mathematically, the main difference between exponentials with real arguments, $e^{-\lambda t}$, and those with imaginary arguments, $e^{i\omega t}$, is that with the former we cannot form an orthogonal basis of functions, whereas such a basis can be formed with the latter. If we depart from our example, we can say that, in general, the response of the network to a step input will be a sum of components that are not orthogonal on each other. The time dependence of these nonorthogonal components can be more complex than an exponential function; they can contain polynomials in time or decaying oscillations, depending on the position in the complex plane of eigenvalues of the transfer matrix H . In contrast, the permanent response obtained from a periodic input is a sum of Fourier components that form an orthogonal set. Orthogonal components are much easier to separate than nonorthogonal ones. This mathematical difference explains the advantage of using oscillatory inputs. However, an argument can be made that increasing the number of replicates will be enough to separate the step response from noise. In what follows we study how many replicates are needed to successfully fight the experimental noise. We will show that fewer replicates are needed if the genetic network is probed with an oscillatory generator rather than a step signal. To keep the argument simple, we will study the difficulty of separating nonorthogonal components for a network for which the response to a step stimulus is a sum of decaying exponentials. The argument can be extended to other types of nonorthogonal components, but this line of thought falls outside the scope of this article. The measured data being a superposition of exponential terms can be written as:

$$f(t) = \int_{x_1}^{x_2} S(x)K(xt)dx, \quad [4]$$

with $K(xt) = e^{-ixt}$ for the periodic response and $K(xt) = e^{-xt}$ for the step stimulus. The spectral function $S(x)$ depends on the network's parameters and the type of the input signal. For example, the spectrum of the autoregulatory system for a periodic input is $S(x) = S_0\delta(x) + S_1\delta(x - i\omega) + S_1^*\delta(x + i\omega)$, where $\delta(x)$ is the Dirac delta function. The coefficients S_0 , S_1 take specific values if the spectrum refers to mean mRNA, proteins, or their correlations. For example, for the protein fluctuation:

$$S_0 = X_{p,0} = \frac{k_p^2 k_0 (\gamma_p - h) \gamma_r}{\omega_0^4 \omega_1}, \quad [5]$$

$$S_1 = X_{p,1} = \frac{ia(-i\gamma_p + \omega + ih)(\omega - 2i\gamma_r)k_p^2}{(\omega^2 - \omega_0^2 - i\omega\omega_1)(\omega^2 - 2i\omega\omega_1 - 4\omega_0^2)(\omega - i\omega_1)}. \quad [6]$$

A detailed description of the spectrum for an autoregulatory network is given in *Supporting Text*. For oscillatory inputs that are not pure cosine function and for more complicated networks, the spectrum is more complex, but is still connected with the measured data like in 4. The spectrum $S(x)$ carries information about the parameters of the genetic network and can be recovered from the data $f(t)$. The network's parameter can be estimated from the spectrum once a model of the network is chosen. Our goal is to show that the spectrum obtained from an oscillatory input signal is much less distorted by the experimental noise than the spectrum obtained from a step input. Laboratory measurements are samples of $f(t)$ at N discrete time points. Given a finite number N of measured data points, f_1, \dots, f_N , the spectrum for the periodic case $S(x)$ can only be approximated as a weighted sum of N terms (*Supporting Text*): $S(x) = \sum_{k=1}^N (s_k + \varepsilon_k/\beta_k)\Theta_k(x)$. Each term, $(s_k + \varepsilon_k/\beta_k)\Theta_k(x)$, contains a function $\Theta_k(x)$ that does not depend on the measured data and the weights $s_k + \varepsilon_k/\beta_k$ that are computed from the measured data f_1, \dots, f_N . In the absence of experimental noise, $\varepsilon_k = 0$, all N coefficients s_k can be computed from the measured data. When experimental noise is present, $\varepsilon_k \neq 0$, what we compute from measured data is $s_k + \varepsilon_k/\beta_k$, and we cannot separate s_k from it because we do not know the actual value for ε_k . The best we can do is to use only those terms for which $s_k > \varepsilon_k/\beta_k$, so the effect of the distortion on s_k is not large. Unfortunately, the distortion increases as β_k gets smaller, which actually happens when k increases. A term can be recovered from noise if $\beta_k^{-1} < s_k/\varepsilon_k$. Usually, this relation is valid for $k = 1 \dots J_p$, with J_p being the last term that can be recovered. A similar relation holds for the exponential case, with α_k instead of β_k and J_e instead of J_p . It is desirable that both cutoffs (J_p, J_e) be as close as possible to the number of sampled points, N . The striking difference between the two cases is that the cutoff J_p is much larger than the cutoff J_e . This difference is a consequence of the fact that the numbers α_k decrease exponentially to 0 (22), whereas β_k stays close to 1 for many k before eventually dropping close to zero (23). This huge difference between α_k and β_k has its origin in the fact that the set of functions of time, $\exp(-\lambda t)$, indexed by λ , do not form an orthogonal set, whereas the functions $\exp(i\omega t)$, indexed by ω , are orthogonal.

In theory, however, we can still hope that a step stimulus can deliver good estimates if the noise ε_k is reduced by using r replicates ($\varepsilon_k \rightarrow \varepsilon_k/\sqrt{r}$). This is not the case. Fig. 4 represents the number of replicates needed to recover the component J_e or J_p if the signal-to-noise ratio (SNR) is 10 ($\text{SNR} \equiv s_{J_e}/\varepsilon_{J_e} = s_{J_p}/\varepsilon_{J_p} = 10$). The number of replicates grows very fast in the exponential case (for $\text{SNR} = 10$ and $N = 20$ we need 269 replicates for the fourth spectral component), whereas in the periodic case, the number of replicates stays low for many spectral components (only for the 17th component it raises to 14,

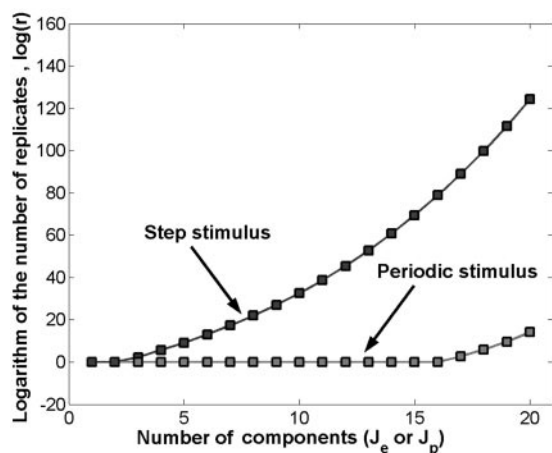


Fig. 4. The number of replicates needed to recover a given spectral component is shown.

with $\text{SNR} = 10$ and $N = 20$). See also Fig. 5, which is published as supporting information on the PNAS web site.

Conclusions and Discussions

We studied the response of a linear stochastic genetic network to an input stimulus (signal). We provide a general formula that relates the mean and covariance matrix of mRNAs and proteins to the input generators. The particular type of periodic signals was studied in detail for an autoregulatory system. We found that fluctuation resonance can manifest in such systems. Besides interesting physical phenomena that can be detected with a periodic signal, the oscillatory input is useful for experimental noise rejection. We compared two experimental designs: one that uses a step stimulus as a perturbation and another that uses a periodic input. We concluded that the response of the genetic network to a periodic stimulus is much easier to detect from noise than the response of the same network to a step stimulus. This conclusion applies whenever the response of the network to an oscillatory input is a sum of Fourier components and can be the case for many nonlinear networks. However, the input-output relations, 1 and 2, apply only to a linear stochastic model. A linear model is a good approximation around a steady state of the genetic network. A genetic network is a nonlinear system and can have several steady states. If the signal generator does not vary in time, the genetic network will be characterized by one of these steady states. When the signal generator starts to oscillate with an amplitude that doesn't drive the network faraway from its steady state, the linear model is a good approximation. For large amplitudes, the nonlinear effects start to be important, and at some values of the generator's amplitude, the network will jump close to a different steady state. Such nonlinear behaviors cannot be described by a linear model. Also, the parameters that describe the network are supposed to be constant in time. This approximation is valid if the changes in the network parameters are slow with respect to the changes produced by the oscillatory input signals. The input frequency should be chosen so that the system can be considered with constant coefficients for the elapsed time of measurements. Also, the period of oscillations must be less than the trend effects caused by growth, apoptosis, etc. Besides biological effects that span large intervals of time, experimental artifacts, like medium evaporation, can superimpose a trend on the measured profile. The input period should be less than the time characteristics of these trends. These trends will impose a limit for the lower range of the input frequencies. The response to oscillations also depends on the time characteristics of the system under study. If the system has a high

damping factor, the high frequencies will be strongly attenuated and the output signal is not measurable. With all of these restrictions, the experimentalist still has the freedom to work in a frequency band, a freedom not present in the step stimulus.

A different line of thought emerges when it comes to analyzing whether the oscillatory method can be scaled to large networks. Experimentally, using high-throughput measurements (microarray and proteomic tools), a large set of gene products can simultaneously be measured. The experimentalist is searching for a pathway that is controlled by a gene. Using oscillatory signals to stimulate the desired gene, the time variation of the downstream genes will contain in its spectrum the input frequency, so these genes will be detected. Moving the signal generator along the pathway, more and more local patches of the network will be uncovered. The global view of the network will consist of all of these patches connected together. The theoretical framework for connecting a set of patches is unclear at present. Experimentally, however, we verified that a source of oscillations propagates into a large genetic network (6). Specifically, a microarray experiment was conducted on mice entrained for 2 weeks on a 24-h period of light/dark signals. The periodic input signal was not implemented at the level of gene promoter; it was an exterior periodic source of light that entrained the internal clock of the cell. After entrainment, and in complete darkness, the output signals (mRNA) were measured every 4 h for 2 days with an Affymetrix (Santa Clara, CA) platform. From $\approx 6,000$ expressed genes in heart, ≈ 500 showed a mRNA that oscillates within a 24-h period. The same results were reported in ref. 24. The next step is to implement the generator at the gene promoter level and measure the spread of the input signal into the network.

Given the advantages of a periodic stimulus presented above, we believe that the experimental implementation of a periodic generator at the promoter level will prove fruitful in the study of genetic networks.

Appendix

The genetic network is described by a linear stochastic network (13–15). The network is driven by using signal generators placed inside the promoters of a subset of genes that are part of the network. For a gene we will denote by D , r , and p the number of DNA, mRNA, and protein molecules, respectively, per cell. We consider r, p to be variables but D to be a constant, and we normalize it to $D = 1$. The state of a cell that contains n active genes is specified by: $\vec{q} = (D_1, D_2, \dots, D_n, r_1, r_2, \dots, r_n, p_1, p_2, \dots, p_n)$. The genetic state is changing in time; for a short transition time, dt , only one \vec{q}_i changes its value, and this new value can be either $\vec{q}_i + 1$ or $\vec{q}_i - 1$. We consider in this article a linear stochastic genetic network characterized by the following transition probabilities: $T(\vec{q}; \vec{q} + 1; t) = \sum_{j=1}^M \tilde{A}_{ij} \vec{q}_j dt$, $T(\vec{q}; \vec{q} - 1; t) = \sum_{j=1}^M \tilde{\Gamma}_{ij} \vec{q}_j dt$. Here \vec{q} is the initial state and $\vec{1}_i$ is a vector of length M with all elements 0 except the one in the position i that is 1. The time variation of the generators that drives gene expression is encapsulated in the matrix \tilde{A}_{ij} , which governs the production of different molecules. The matrices \tilde{A}_{ij} and $\tilde{\Gamma}_{ij}$ consist of four submatrices, corresponding to splitting the state \vec{q} into two subgroups. One subgroup contains only the DNA states (D_1, \dots, D_n) and the other subgroup contains the protein and mRNA states $q = (r_1, r_2, \dots, r_n, p_1, p_2, \dots, p_n)$,

$$\tilde{A} = \begin{bmatrix} 0 & 0 \\ \text{Gen} & A \end{bmatrix}, \quad \tilde{\Gamma} = \begin{bmatrix} 0 & 0 \\ 0 & \Gamma \end{bmatrix}. \quad [7]$$

The generator submatrix Gen has a special form. It is a $2n \times n$ matrix and locates the position of the generators in the genetic network: $\text{Gen}_{ij} = g_i(t) \delta_{ij}$, $i = 1 \dots 2n$, $j = 1, \dots, n$. Each gene promoter is driven by one generator $g_i(t)$, $i = 1, \dots, n$, which will influence the mRNA production of gene i . The same

mRNA production can be influenced by the protein concentration, and this feedback effect is described by the elements of the $2n \times 2n$ matrix A (7). The structure of the matrix A is a consequence of the topology of the genetic network. The equation for the probability $P(\tilde{q}, t)$ of the network to be in the state \tilde{q} at time t is: $\partial P(\tilde{q}, t)/\partial t = \sum_{i=1}^M (E_i^- - 1) \sum_{k=1}^M \tilde{A}_{ik} \tilde{q}_k P(\tilde{q}, t) + \sum_{i=1}^M (E_i^+ - 1) \sum_{k=1}^M \tilde{\Gamma}_{ik} \tilde{q}_k P(\tilde{q}, t)$, where the shift operators E_i^\pm are given by $E_i^\pm P(\tilde{q}, t) = P(\tilde{q}, \dots, \tilde{q}_i \pm 1, \dots, \tilde{q}_M)$.

We need the time evolution equations for mRNAs and proteins: $\mu_i = \langle q_i \rangle$ and $\nu_{ij} = \langle q_i q_j \rangle - \langle q_i \rangle \langle q_j \rangle$, $i, j = 1, \dots, 2n$. In matrix notation, for the column vector μ and for the matrix X with elements given by $X_{ij} = \nu_{ij} - \delta_{ij} \mu_i$ we obtain:

$$\frac{d}{dt} = H\mu + G, \quad [8]$$

$$\frac{d}{dt} X = HX + HT^T + H \text{diag}(\mu) + \text{diag}(\mu)H^T + 2\text{diag}(\Gamma\mu). \quad [9]$$

Here H^T is the transpose matrix of $H = A - \Gamma$ and $\text{diag}(\mu)$ has nonzero elements only on the principal diagonal: $\text{diag}(\mu)_{ij} =$

$\delta_{ij} \mu_i$. Using the Laplace transform, the solution to 8 is 1. Eq. 9 is a matrix equation. To solve this equation we first transform it to an equation where the unknown is a column vector. The transformation needed is $X \rightarrow \text{vec}(X)$, where the column vector $\text{vec}(X)$ contains the columns of the matrix X one on top of the other, starting with the first column and ending with the last column. The vec mapping has the useful property that $\text{vec}(HX) = (1 \otimes H)\text{vec}(X)$, $\text{vec}(XH) = (H^T \otimes 1)\text{vec}(X)$, where 1 is the unit matrix and $A \otimes B$ is the tensor product of matrices A and B . The column vector $\text{vec}(\text{diag}(\mu))$ can be expressed in terms of the column vector μ : $\text{vec}(\text{diag}(\mu)) = L\mu$, where L is a lift matrix from a space of dimension of μ to the square of this dimension: $L = (P_1, \dots, P_{2n})^T$, $(P_k)_{ij} = \delta_{ik} \delta_{jk}$. The solution to 9 takes the form 2.

We thank Kai-Florian Storch for valuable discussions about the experimental design of the periodic generator, Charles J. Weitz for pointing out to us the *CryI*,2 mutant experiments, and the reviewers for their comments. Our work was created and developed independently of ref. 25, which was brought to our attention by one reviewer in December 2004. O.L. is grateful to his colleagues at the Center for Biotechnology and Genomic Medicine for their encouragement. This work was supported in part by National Institutes of Health Grant 1R01HG02341 and National Science Foundation Grant DMS-0090166.

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